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(54) **BONE SCREW DRIVER**

(75) Inventors: **Ernie Corrao**, Bethel, CT (US);
Rebecca H. Wahl, Escondido, CA (US);
Louise M. Focht, Del Mar, CA (US)

(73) Assignee: **Tornier, Inc.**, Edina, MN (US)

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81/453; 411/2-7, 39, 410
See application file for complete search history.

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DePuy FRSTM—Fusion and Reconstruction System, © DePuy, a Johnson & Johnson company 2005-2006.

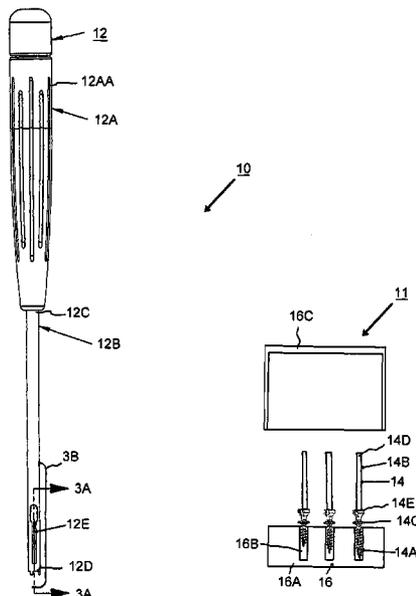
* cited by examiner

Primary Examiner — Thomas C Barrett
Assistant Examiner — Christian Sevilla
(74) *Attorney, Agent, or Firm* — Faegre & Benson LLP

(57) **ABSTRACT**

A bone screw driver (12) for inserting a bone screw (14) into a bone region (218A) includes a driver shaft (12B) that selectively engages the bone screw (14). The bone screw (14) includes a screw threaded region (14A) and a screw engagement region (14B). The screw engagement region (14B) includes a screw shaft (14D) and an engager ring (14E). The driver shaft (12B) includes a shaft aperture (322), a first resilient member (324A), and a first shaft projection (326A). The shaft aperture (322) receives at least a portion of the screw shaft (14D), the first resilient member (324A) engages the screw shaft (14D) to inhibit movement of the screw shaft (14D), and the first shaft projection (326A) engages the engager ring (14E) so that rotation of the driver shaft (12B) results in rotation of the bone screw (14). With this design, in certain embodiments, the bone screw (14) can be removed with the bone screw driver (12) from a screw retainer (16) that retains the bone screw (14), and inserted into the bone region (218A) without the physician contacting with the bone screw (14). This reduces the likelihood of contaminating the bone screw (14) and increases the likelihood of success for the procedure.

10 Claims, 4 Drawing Sheets



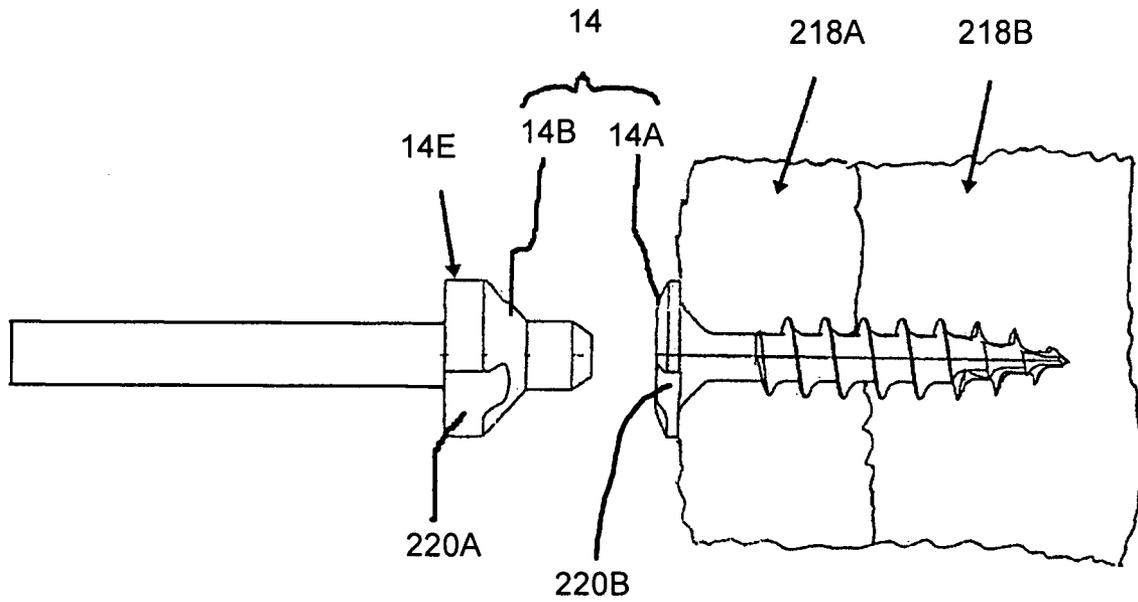


Figure 2A

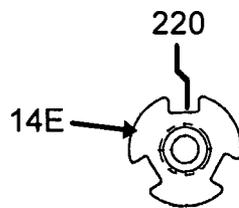


Figure 2B

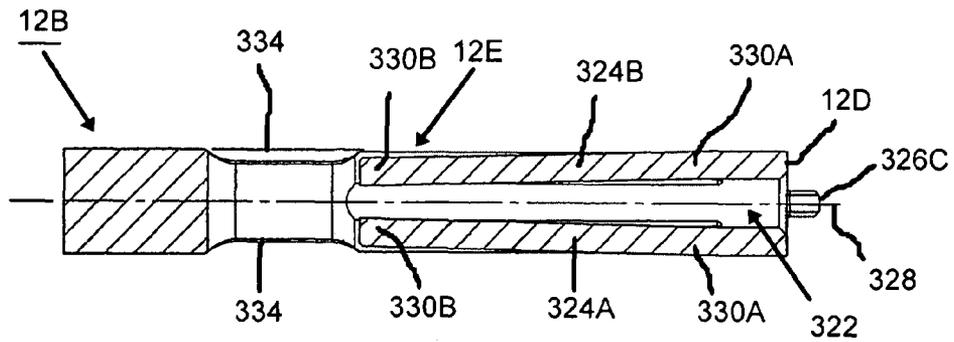


Figure 3A

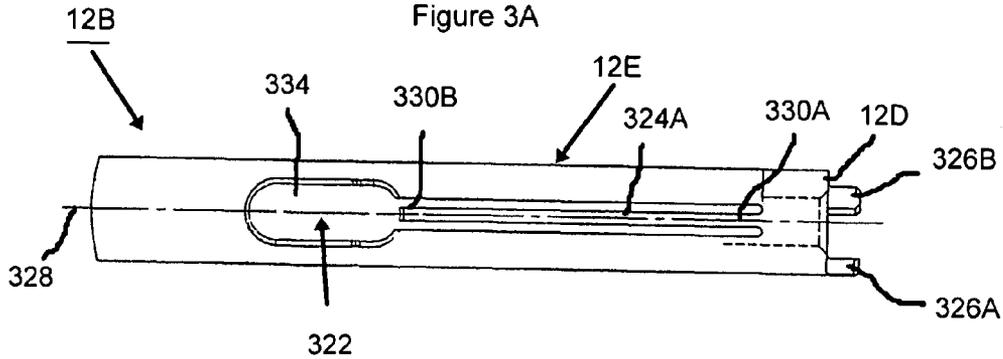


Figure 3B

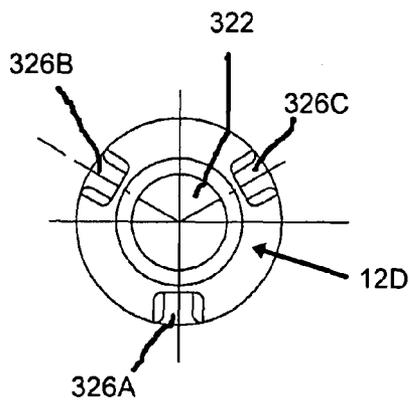


Figure 3C

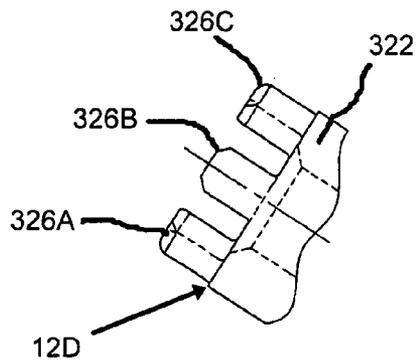


Figure 3D

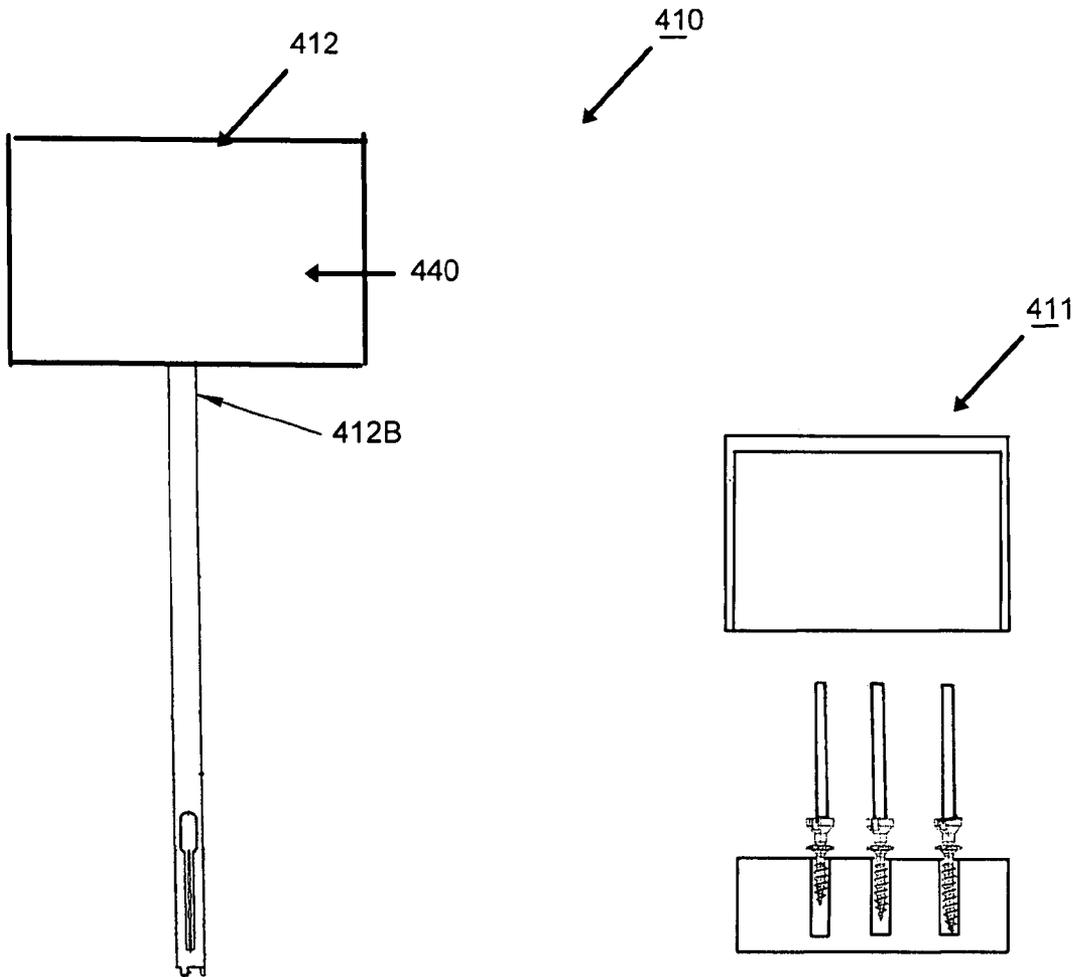


Figure 4

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BONE SCREW DRIVER

BACKGROUND

It is often necessary to fuse two bone regions together to repair a fracture or to fuse a joint. One type of device used to fuse two bone regions is a bone screw than is threaded into the bone regions with a bone screw driver by a physician. Because the size and orientation of the bone regions that need to be fused can vary greatly, the bone screws are designed in varying lengths and diameters. For any particular bone fusing procedure, the size of the bone screw must be chosen properly so as to maximize the stability of the bone regions after they are fused together, and to minimize the irritation adjacent to the area where the bone screw has been inserted.

Often the physician is provided with a container that contains a plurality of alternatively sized bone screws. With this system, the physician can select the bone screw from the container that is appropriate for the procedure being performed.

It should be noted that it is important to keep the bone screw sterile. Accordingly, it is desired to minimize human contact with the bone screw prior to insertion into the bone regions.

SUMMARY

The present invention is directed toward a bone screw driver for inserting a bone screw into a bone region. The bone screw includes a screw threaded region and a screw engagement region. The screw engagement region includes a screw shaft and an engager ring. The bone screw driver includes a driver handle and a driver shaft that is coupled to the driver handle. The driver shaft includes a shaft aperture, a first resilient member, and a first shaft projection. The shaft aperture receives at least a portion of the screw shaft, the first resilient member engages the screw shaft to inhibit movement of the screw shaft, and the first shaft projection engages the engager ring so that rotation of the driver shaft results in rotation of the bone screw. With this design, in certain embodiments, the bone screw can be removed with the bone screw driver from a screw retainer that contains the bone screw, and inserted into the bone region without the physician directly contacting the bone screw. This reduces the likelihood of contaminating the bone screw and increases the likelihood of success for the procedure.

In one embodiment, the first resilient member extends into the shaft aperture to contact the screw shaft. For example, the first resilient member can cantilever into the shaft aperture to contact the screw shaft. Additionally, the driver shaft can include a second resilient member that extends into the shaft aperture to contact the screw shaft.

Further, in one embodiment, the driver shaft includes a second shaft projection and a third shaft projection that engage the engager ring so that rotation of the driver shaft results in rotation of the bone screw.

Additionally, the present invention is directed to a combination that includes a one or more bone screws, a screw retainer that retains the one or more bone screws, and a bone screw driver as detailed above.

Moreover, the present invention is directed to a method for inserting a bone screw into a bone region. The method including the steps of engaging the bone screw with the driver shaft and rotating the driver shaft and the bone screw to thread the bone screw into the bone region. In this design, the driver shaft can have similar features as detailed above.

BRIEF DESCRIPTION OF THE DRAWINGS

The novel features of this invention, as well as the invention itself, both as to its structure and its operation, will be best

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understood from the accompanying drawings, taken in conjunction with the accompanying description, in which similar reference characters refer to similar parts, and in which:

FIG. 1 is a simplified side view of a bone screw assembly in partial cut-away and a bone screw driver having features of the present invention;

FIG. 2A is a simplified side view of a pair of bone regions, in cut-away, that are fused together with a snap-off bone screw in a decoupled configuration;

FIG. 2B is a simplified top view of the bone screw of FIG. 2A;

FIG. 3A is a cut-away view taken on line 3A-3A in FIG. 1;

FIG. 3B is an enlarged view of a portion of the bone screw driver taken from FIG. 1;

FIG. 3C is an end view of the portion of the bone screw driver of FIG. 3B;

FIG. 3D is a perspective view of the end of the bone screw driver; and

FIG. 4 is a simplified side view of the bone screw assembly in partial cut-away and another embodiment of a bone screw driver having features of the present invention.

DESCRIPTION

FIG. 1 illustrates a combination 10 including a bone screw assembly 11 and a bone screw driver 12 having features of the present invention. The bone screw assembly 11 includes one or more bone screws 14 and a screw retainer 16 that retains the one or more bone screws 14. As an overview, in certain embodiments, the bone screw driver 12 can be used by a physician (not shown) to remove one of the bone screw 14 from the screw retainer 16, and insert the bone screw 14 into one or more bone regions 218A, 218B (illustrated in FIG. 2A) without the physician directly contacting the bone screw 14. This reduces the likelihood of contaminating the bone screw 14 and increases the likelihood of success for the procedure.

The number and design of the bone screws 14 in the bone screw assembly 11 can be varied to achieve the desired range of surgery options. In FIG. 1, the bone screw assembly 11 includes three, bone screws 14. Alternatively, the bone screw assembly 11 could have more than three or less than three bone screws 14. Typically, the number of alternatively sized bone screws 14 is greater than three so that the physician has a large choice of possible bone screws 14 for the procedure.

In FIG. 1, each of the bone screws 14 includes a screw threaded region 14A, and a screw engagement region 14B. The screw threaded region 14A is threaded into one or more of the bone regions 218A, 218B, and the screw engagement region 14B is engaged by the bone screw driver 12 to rotate the bone screw 14 during insertion of the screw threaded region 14A into one or more of the bone regions 218A, 218B. The design and size of the screw threaded region 14A and the screw engagement region 14B of each bone screw 14 can vary according to the desired use for the bone screw assembly 11. In FIG. 1, each of the screw threaded regions 14A has a somewhat similar thread pattern and a different thread length. With this design, the physician can select the bone screw 14 with the desired thread length for the operation. Alternatively, the thread pitch, width or design can be different for each of the bone screws 14.

Additionally, in FIG. 1, each of the screw threaded regions 14A includes a screw head 14C that engages one of the bone regions 218A, 218B when the bone screw 14 is fully inserted.

Further, in FIG. 1, the screw engagement region 14B for each of the bone screws 14 is substantially similar. In this embodiment, the screw engagement region 14B includes a screw shaft 14D and an engager ring 14E. The shaft 14D is

engaged by the bone screw driver 12 to retain the bone screw 14 during removal from the screw retainer 16 and insertion into the bone regions 218A, 218B, while the engager ring 14E is engaged by the bone screw driver 12 to rotate the bone screw 14.

In FIG. 1, the shaft 14D has generally right cylindrical shape and has a generally circular cross-section. Alternatively, the shaft 14D can have another configuration. For example, the shaft 14D can have an octagonal or rectangular shaped cross-section.

Further, in FIG. 1, the engager ring 14E is somewhat disk shaped and is located near the screw threaded region 14A. The engager ring 14E is described in more detail below.

The type of material utilized in the bone screws 14 can be varied to meet the requirements of the one or more bone regions 218A, 218B. For example, the bone screws 14 can be formed from titanium, stainless steel, or a bio-absorbable material.

The length and cross-section of screw threaded regions 14A and the screw engagement regions 14B can be varied to suit the procedure being performed on the patient. In one non-exclusive embodiment, the screw threaded regions 14A has a length of between approximately eleven and seventeen millimeters, and the screw engagement region 14B has a length of between approximately ten and twenty millimeters. However, greater or lesser lengths can be utilized.

The screw retainer 16 retains the bone screws 14 prior to the particular bone screw 14 being selected by the physician. In FIG. 1, the screw retainer 16 is designed to retain three, bone screws 14 and includes a retainer base 16A having three screw receivers 16B, e.g. apertures, that retain the bone screws 14 in a spaced apart configuration. Alternatively, the screw retainer 16 could be designed to retain more than three or less than three bone screws 14.

In FIG. 1, the retainer base 16A retains the bone screws 14 with the screw engagement region 14B exposed so that the screw engagement region 14B can be accessed with the bone screw driver 12. With this design, the bone screw driver 12 can be used by the physician to remove the appropriate bone screw 14 from the screw retainer 16, without the physician directly contacting with the bone screw 14.

In one embodiment, the screw retainer 16 maintains the bone screws 14 in a sterile environment. For example, the screw retainer 16 can include a removable, retainer top 16C that can be secured to the retainer base 16A to fully enclose the bone screws 14 in the screw retainer 16.

The bone screw driver 12 selectively retains the selected bone screw 14 so that the bone screw driver 12 can be used to remove the selected bone screw 14 from the screw retainer 16 and so that the bone screw driver 12 can be used to thread the selected bone screw 14 in the bone regions 218A, 218B. In FIG. 1, the bone screw driver 12 includes a handle 12A and a driver shaft 12B that is secured to the handle 12A so that rotation of the handle 12A results in rotation of the driver shaft 12B.

In this embodiment, the handle 12A is sized and shaped to be moved and rotated with a hand of the physician. In FIG. 1, the handle 12A is generally cylindrical shaded and is shaped somewhat similar to the handle of a screwdriver. The handle 12A can include a plurality of handle slots 12AA to facilitate gripping of the handle 12A with the human hand. Alternatively, for example, the handle 12A can have a "T" shaped configuration.

Suitable materials for the handle 12A include plastic (e.g. polyphenylsulfone sold under the trademark Radel), and metal such as aluminum or stainless steel. In one embodiment, the handle 12A is molded onto a portion of the driver

shaft 12B. Alternatively, the handle 12A can be secured with an adhesive or pinned mechanically to the driver shaft 12B.

The driver shaft 12B is generally rigid and includes a proximal end 12C that is secured to the handle 12A, an opposed distal end 12D, and a screw engager assembly 12E located near the distal end 12D that engages the screw engagement region 14B of the selected bone screw 14. In FIG. 1, the driver shaft 12B has a generally cylindrical shaped and a generally circular cross-section. Alternatively, the driver shaft 12B can have another configuration. For example, the driver shaft 12B can have an octagonal or rectangular shaped cross-section.

In one embodiment, the driver shaft 12B is integrally formed as a unitary structure. Alternatively, portions of the driver shaft 12B can separately formed and joined together during manufacturing. A non-exclusive example of a suitable material for the driver shaft 12B is stainless steel. In one non-exclusive embodiment, the driver shaft 12B extends approximately 3.5 inches below the handle 12A.

The screw engager assembly 12E is designed to engage the bone screw 14 to facilitate removal of the selected bone screw 14 from the screw retainer 16 and insertion of the bone screw 14 in the patient. With this design, the physician can use the bone screw driver 12 to remove the appropriate bone screw 14 from the screw retainer 16, and insert the bone screw 14 into one or more bone regions 218A, 218B without the physician directly contacting with the bone screw 14. The screw engager assembly 12E is discussed in more detail below.

FIG. 2A is a simplified side illustration of a bone screw 14 that has been inserted into a first bone region 218A and a second bone region 218B of a human. In this embodiment, the bone screw 14 urges the bone regions 218A, 218B together so that the bone regions 218A, 218B are fused together. The type and location of the bone regions 218A, 218B urged together can vary. For example, the bone screw 14 can be used to fuse a fracture of a human bone, to immobilize and fuse a human joint, or to fuse together adjacent bones. Alternatively, for example, one or more of the bone screws 14 can be used to secure a plate (not shown) or other device to one or more bone regions 218A, 218B.

Additionally, FIG. 2A illustrates that the bone screw 14 is a snap-off type screw, in which the screw engagement region 14B is designed to break away from the screw threaded region 14A after the screw threaded region 14A has been threaded into the bone regions 218A, 218B. Alternatively, the bone screw 14 could have a different design.

It should be noted that in certain embodiments, the bone screw driver 12 (illustrated in FIG. 1) continues to retain the screw engagement region 14B after the screw engagement region 14B has broken away from the screw threaded region 14A. This reduces the likelihood that the screw engagement region 14B will be misplaced.

It should be noted that the bone screw 14 can be inserted with a pilot hole (not shown) or without a pilot hole, depending upon the condition and type of the one or more bone regions 218A, 218B. In one embodiment, the bone screw 14 is self drilling and/or tapping.

FIGS. 2A and 2B illustrate the engager ring 14E in more detail. The design of the engager ring 14E can be varied to achieve the desired area to be engaged by the bone screw driver 12. In FIGS. 2A and 2B, the engager ring 14E is somewhat cylindrical disk shaped and includes a plurality of spaced apart, circumferentially distributed ring notches 220A. The ring notches 220A allow for engagement by the screw engager assembly 12E of the bone screw driver 12 so that rotation of the bone screw driver 12 results in rotation of the bone screw 14. In FIGS. 2A and 2B, the engager ring 14E

includes three spaced apart ring notches **220A** that are approximately 120 degrees apart. Alternatively, the engager ring **14E** can be designed to have more than three or less than three ring notches **220A**. Alternatively, the engager ring **14E** can have another configuration. For example, the edges of the ring notches **220A** can be rounded to be more tissue friendly.

Additionally, the screw threaded region **14A** can include a head that is somewhat cylindrical disk shaped and includes a plurality of spaced apart, circumferentially distributed head notches **220B**. The ring notches **220B** allow for engagement by the screw engager assembly **12E** of the bone screw driver **12** so that the screw threaded region **14A** can be further inserted or removed after the screw engagement region **14B** has broken away from the screw threaded region **14A**. In FIG. **2A**, the head includes three spaced apart head notches **220B** that are approximately 120 degrees apart. Alternatively, the head can be designed to have more than three or less than three head notches **220B**.

FIG. **3A** is a cut-away view and **3B** is a side view of the screw engager assembly **12E** of the driver shaft **12B**. In this embodiment, the driver shaft **12B** includes a shaft aperture **322**, a first resilient member **324A**, a second resilient member **324B**, a first shaft projection **326A**, a second shaft projection **326B**, and a third shaft projection **326C** that cooperate to form the screw engager assembly **12E**. Alternatively, the screw engager assembly **12E** can have an alternative configuration. For example, the screw engager assembly **12E** can have more than two or fewer than two resilient members **324A**, **324B**, and/or more than three or fewer than three shaft projections **326A**, **326B**, **326C**.

The shaft aperture **322** receives at least a portion of the screw shaft **14D** (illustrated in FIG. **1**). In FIGS. **3A** and **3B**, the shaft aperture **322** is a generally cylindrical shaped opening that extends into a portion of the driver shaft **12B** from the distal end **12D** along a longitudinal axis **328** of the driver shaft **12B**. In one embodiment, the shaft aperture **322** has a diameter that is slightly greater than the diameter of the screw shaft **14D**. In one non-exclusive embodiment, the shaft aperture **322** has an aperture depth of between approximately eleven and twelve centimeters.

The resilient members **324A**, **324B** engage the side of the screw shaft **14D** when the screw shaft **14D** is inserted into the shaft aperture **322** to inhibit movement of the screw shaft **14D** from the shaft aperture **322**. In FIGS. **3A**, and **3B**, each of the resilient members **324A**, **324B** is a generally rectangular shaped beam that extends into the shaft aperture **322** to contact the screw shaft **14D**. For example, each of the beams **324A**, **324B** can cantilever into the shaft aperture **322** to contact the side of the screw shaft **14D**. In this embodiment, each of the beams **324A**, **324B** includes an attached end **330A** that is attached to the rest of the driver shaft **12B** near the distal end **12D**, and a cantilevering end **330B** that cantilevers into the shaft aperture **322**. In one embodiment, the beams **324A**, **324B** are formed by cutting slots **332** in the driver shaft **12B** to form the beams **324A**, **324B** and subsequently deforming the beams **324A**, **324B** to cantilever inward.

In FIGS. **3A** and **3B**, the distance between the cantilevering ends **330B** is less than the diameter of the shaft aperture **322** and the diameter of the screw shaft **14D**. As a result thereof, the cantilevering ends **330B** engage the sides of the screw shaft **14D** when the screw shaft **14D** is inserted into the shaft aperture **322**, and the friction between the cantilevering ends **330B** and the screw shaft **14D** inhibit the screw shaft **14D** from being removed from the shaft aperture **322**.

Alternatively, one or more of the resilient members **324A**, **324B** can have a design that is different than that illustrated

herein. For example, one or more of the resilient members **324A**, **324B** can be a spring positioned in the shaft aperture **322** that extends inward.

Additionally, the driver shaft **12B** can include one or more side apertures **334** that facilitate manufacturing of the driver shaft **12B**.

The shaft projections **326A**, **326B**, **326C** engage the notches **220** (illustrated in FIG. **2B**) of the engager ring **14E** (illustrated in FIG. **2B**) so that rotation of the driver shaft **12B** results in rotation of the bone screw **14**. The design of the shaft projections **326A**, **326B**, **326C** can vary according to the design of the notches **220**. FIGS. **3C** and **3D** illustrate the shaft projections **326A**, **326B**, **326C** in more detail. In this embodiment, each of shaft projections **326A**, **326B**, **326C** is a generally rectangular beam with tapered edges, that cantilevers away from the distal end **12D**. Further, the spaced apart shaft projections **326A**, **326B**, **326C** are distributed circumferentially and are positioned around the opening to the shaft aperture **322** at approximately 120 degrees relative to each other.

In one non-exclusive embodiment, each of the shaft projections **326A**, **326B**, **326C** extends between approximately 1 and 1.5 millimeters.

As stated above, the bone screw driver **12** can be used by a physician to remove one of the bone screws **14** from the screw retainer **16**, and insert the bone screw **14** into one or more bone regions **218A**, **218B** without the physician directly contacting with the bone screw **14**. More specifically, after the physician determines the appropriate bone screw **14**, the physician moves the bone screw driver **12** so that the shaft aperture **322** receives the screw shaft **14D**. Further, the bone screw driver **12** is moved downward and rotated until the shaft projections **326A**, **326B**, **326C** are positioned in the notches **220**. In this position, the resilient members **324A**, **324B** engage the side of the screw shaft **14D** and the shaft projections **326A**, **326B**, **326C** engage the notches **220**. As a result thereof, the bone screw driver **12** can be used by a physician to remove the bone screw **14** from the screw retainer **16**, and insert the bone screw **14** into one or more bone regions **218A**, **218B**. Stated in another fashion, the user can easily couple the bone screw driver **12** to the desired bone screw **14**, with one hand, without the need of touching or otherwise handling the individual bone screw **14**. This feature enables the user to maintain the screw **14** in the most clean and sterile condition possible before inserting the screw **14**.

FIG. **4** illustrates another embodiment of a combination **410** including a bone screw assembly **411** and a bone screw driver **412** that are somewhat similar to the bone screw driver **12** described above. However, in this embodiment, the bone screw driver **412** includes an electric motor **440** instead of a handle **12A** (illustrated in FIG. **1**) to electrically rotate the driver shaft **412B**.

While the bone screw driver **12**, as shown and disclosed herein is fully capable of obtaining the objects and providing the advantages herein before stated, it is to be understood that it is merely illustrative of the presently preferred embodiments of the invention and that no limitations are intended to the details of construction or design herein shown other than as described in the appended claims.

What is claimed is:

1. A bone screw driver for inserting a bone screw into a bone region, the bone screw including a screw threaded region and a screw engagement region, the screw engagement region including a screw shaft and an engager ring, the bone screw driver comprising:
a driver handle;

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a driver shaft coupled to the driver handle, the driver shaft including a shaft aperture for receiving at least a portion of the screw shaft, a first resilient member that engages the screw shaft to inhibit movement of the screw shaft, and a first shaft projection that engages the engager ring so that rotation of the driver shaft results in rotation of the bone screw; and a bone screw including a screw threaded region and a screw engagement region, the screw engagement region including a screw shaft and an engager ring; wherein the screw engagement region is in snap-off engagement with the screw threaded region in which the screw engagement region breaks away from the screw threaded region after the screw threaded region has been threaded into bone; wherein the first resilient member cantilevers into the shaft aperture to contact the screw shaft.

2. The bone screw driver of claim 1 wherein the driver shaft includes a second resilient member that extends into the shaft aperture to contact the screw shaft.

3. The bone screw driver of claim 2 wherein the driver shaft includes a second shaft projection and a third shaft projection that engage the engager ring so that rotation of the driver shaft results in rotation of the bone screw.

4. The bone screw driver of claim 1 wherein the driver shaft includes a second shaft projection and a third shaft projection that engage the engager ring so that rotation of the driver shaft results in rotation of the bone screw.

5. A combination comprising:

a bone screw adapted for insertion into a bone region, the bone screw including a screw threaded region and a screw engagement region, the screw engagement region including a screw shaft and an engager ring; and

a bone screw driver for inserting the bone screw into the bone region, the bone screw driver including a driver shaft having a shaft aperture for receiving at least a portion of the screw shaft, a first resilient member that engages the screw shaft to inhibit movement of the screw shaft, and a first shaft projection that engages the engager ring so that rotation of the driver shaft results in rotation of the bone screw; wherein the screw engagement region is in snap-off engagement with the screw

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threaded region in which the screw engagement region breaks away from the screw threaded region after the screw threaded region has been threaded into bone; wherein the first resilient member cantilevers into the shaft aperture to contact the screw shaft.

6. The combination of claim 5 wherein the driver shaft includes a second resilient member that extends into the shaft aperture to contact the screw shaft.

7. The combination of claim 6 wherein the driver shaft includes a second shaft projection and a third shaft projection that engage the engager ring so that rotation of the driver shaft results in rotation of the bone screw.

8. The combination of claim 5 wherein the driver shaft includes a second shaft projection and a third shaft projection that engage the engager ring so that rotation of the driver shaft results in rotation of the bone screw.

9. The combination of claim 5 further comprising a screw retainer that selectively retains the bone screw with the screw engagement region exposed.

10. A combination comprising:

a bone screw adapted for insertion into a bone region, the bone screw including a screw threaded region and a screw engagement region, the screw engagement region in snap-off engagement with the screw threaded region in which the screw engagement region breaks away from the screw threaded region after the screw threaded region has been threaded into bone, the screw engagement region including a screw shaft and an engager ring; and

a bone screw driver for inserting the bone screw into the bone region, the bone screw driver including a driver shaft having a shaft aperture for receiving at least a portion of the screw shaft, a first resilient member that engages the screw shaft to inhibit movement of the screw shaft, and a first shaft projection that engages the engager ring so that rotation of the driver shaft results in rotation of the bone screw; wherein the first resilient member cantilevers into the shaft aperture to contact the screw shaft.

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