Technical Report for H₂O₂-Based N95 Reuse Risk Management

Much of the available literature on decontamination of N95 FFRs reviewed in this document is a result of recent efforts to relieve the shortage of N95 FFRs during the SARS-CoV-2 outbreak. Because of this, many of the research papers cited in this document are not yet peer reviewed. **For clarity, wherever non-peer-reviewed results are cited in this report, the citation is preceded by a ***.

Summary of Updates in v2.0 Report: Update includes more in-depth description of hydrogen peroxide systems, new findings on effects of decontamination on N95 masks inoculated with SARS-CoV-2 (*Kumar et al. 2020; *Oral et al. 2020; *Fischer et al. 2020); and two new FDA EUAs for hydrogen peroxide decontamination methods.

Executive Summary

Hydrogen peroxide is well known for eradicating resistant microorganisms such as *Serratia marcescens, Clostridium botulinum spores and Clostridium difficile*. In vapor or gaseous form, it can be used to decontaminate whole rooms, biosafety cabinets and medical instruments made of metal or plastic. Recent studies demonstrate that hydrogen peroxide vapor decontaminates N95 masks inoculated with SARS-CoV-2 virus with greater than 3-log attenuation. There are many types of hydrogen peroxide delivery systems that vary in humidity, temperature, hydrogen peroxide concentration, and duration of exposure, depending on whether the hydrogen peroxide is delivered as a vapor, aerosol, or ionized gas. This makes it particularly important for hospitals to make sure that the proper protocol for N95 mask decontamination matches the available equipment. For example, the Bioquell process, used by Battelle, will not damage N95 masks with up to 20 repeated decontamination cycles. But the STERRAD (ASP) process will damage N95 filters with very few decontamination cycles. The FDA has granted Emergency Use Authorization for three different hydrogen peroxide decontamination processes for N95 masks, including one mail-out process.

1. Overview

The novel coronavirus (SARS-CoV-2) that causes coronavirus disease 2019 (COVID-19) has led to a global shortage of N95 Filtering Facepiece Respirators (N95 FFRs, also referred to as 'N95 masks'). While new N95 FFRs should be used, in this emergency, it may be necessary to decontaminate FFRs. In this document, we review the use of hydrogen peroxide vapor to decontaminate N95 FFRs with the goal of increasing the useful lifetime of N95 FFRs worn by healthcare providers during the COVID-19 pandemic. Effective decontamination requires inactivation of the SARS-CoV-2 virus and maintenance of both the fit and filtration efficiency of the N95 FFR while minimizing the risk of cross-contamination.

Hydrogen peroxide (H₂O₂) vapor decontamination is an established industrial decontamination method used in hospitals, research settings, research animal facilities, pharmaceutical and medical industries, and by police and fire departments (Mickelsen et al., EPA Report, 2017) for terminal decontamination of biosafety cabinets (BSC) and whole rooms. Hydrogen peroxide vapor/vapor phase hydrogen peroxide (HPV/VPHP or VHPTM), aerosolized hydrogen peroxide (aHP), or hydrogen peroxide gas plasma (HPGP) inactivate highly resistant

pathogens, including nosocomial bacterial spores and viruses. The hydrogen peroxide decontamination method is incompatible with cellulose, which is a component in some N95 FFRs (Appendix A).

A number of studies (Battelle et al., 2016, 2020; Bergman et al., 2010, Viscusi et al., 2009; *Oral et al., 2020) have demonstrated that some N95 FFRs can be safely decontaminated with proper use of HPV/VPHP or VHPTM. Most of these studies used the Bioquell HPV/VPHP or the Sterris VHPTM systems. The Battelle study demonstrated that up to 20 cycles of HPV treatments on N95 FFRs will not compromise filter performance, pressure drop, fit, or elastic band quality. For the purpose of bulk decontamination of N95 FFRs, a whole-room decontamination system with controlled air-flow, allows carts filled with N95 FFRs to be wheeled in and out; see protocol developed by Duke University Medical Center (*Schwartz et al., 2020). This would provide for a capacity of up to 2000 N95 FFRs per day using a 12 x 12 ft room. Alternatively, an air-flow controlled chamber or BSC could be temporarily outfitted with a VHPTM system (e.g., *Oral et al., 2020), which would then have capacity for 100–120 N95 FFRs/cycle, depending on BSC size. The duration of a decontamination cycle varies from 4.5 to 8 hours depending on the system and volume of the chamber or room.

| Method | Abbreviation | Description | Example Providers |
|---|--------------|---|--------------------------------------|
| Hydrogen Peroxide Vapor/Vapor Phase Hydrogen Peroxide | HPV/VPHP | Wet H ₂ O ₂ vapor, >500 ppm | Bioquell (Claris); Battelle CCDS™ |
| Hydrogen Peroxide Gas Plasma | HPGP | HPV, RF, H_2O_2 plasma | ASP (STERRAD™) |
| lonized Hydrogen Peroxide | iHP® | Wet H_2O_2 microdroplets ionization arc | Tomi™ (SteraMist®) |
| Vaporized Hydrogen Peroxide [™] | VHP™ | Dry H ₂ O ₂ vapor, >750 ppm | Steris (ARD) |
| Aerosolized Hydrogen Peroxide | aHP | Wet H_2O_2 microdroplets, 100-120 ppm; additive: silver nitrate (0.01%) | Halosil |
| Aerosolized Hydrogen Peroxide | aHP | Wet H ₂ O ₂ microdroplets, 80-150 ppm | Curis® |

2. Status of Federal Guidance

In this unprecedented COVID-19 pandemic, due to a limited supply of N95 FFRs, the Centers for Disease Control and Prevention (CDC) have provided guidance that healthcare

workers can practice extended use or limited reuse of N95 FFRs (CDC, 2020b). In addition, the CDC has provided guidance to hospitals on methods for decontaminating N95 FFRs during a crisis (CDC, 2020c).

The Occupational Safety and Health Administration (OSHA) states that cosmetics or other barriers should not be present during respirator use (OSHA, n.d.). Emergency use authorizations (EUAs) that the FDA has granted for N95 FFR decontamination during the COVID-19 pandemic also stipulate that cosmetics not be present on respirators sent for decontamination (Battelle, 2020).

After decontamination, the CDC recommends that a 'user seal check' is performed when the respirator is donned to ensure adequate seal (CDC, 2020c). A user seal check after every decontamination cycle is especially important because there is evidence that the fit factor of N95 respirators decreases with numerous don/doffs (Bergman et al., 2012).

Per FDA guidelines for N95 FFR decontamination EUAs, virucidal decontamination requires \geq 3-log reduction (corresponding to a 99.9% reduction) in viral activity (FDA, 2020). Based on this guideline, we describe a process as sufficiently "decontaminating" or "inactivating" only when it leads to a \geq 3-log reduction in viral activity. **Note that our definition of decontamination in this report, unless otherwise specified, only considers virucidal activity and does** *not* **consider mycobactericidal or sporicidal activity**, for which the FDA has other guidelines (FDA, 2020). **N95 FFR decontamination processes for SARS-CoV-2 do not necessarily result in sterilization (killing of all microorganisms) of the N95 FFR**.

The March 31, 2020 CDC guidance on the decontamination and reuse of N95 FFRs includes the use of vaporized H₂O₂ (Decontamination and Reuse of Filtering Facepiece Respirators, 2020). On March 28, 2020 the Battelle HPV/VPHP Critical Care Decontamination System[™] (CCDS) received FDA EUA for decontamination of N95 FFRs for reuse for a maximum of 20 decontamination cycles (single-user reuse or pooled use not specified). Battelle reports that each of their six facilities can process at least 80,000 N95 FFRs per day (Battelle, 2020). On April 9, 2020 the STERIS VHP[™] system (V-PRO, maX, and maX2) received FDA EUA for decontamination of N95 FFRs for a maximum of 10 decontamination cycles. On April 11, 2020 the ASP STERRAD process (100S, NX, 100NX) received FDA EUA for decontamination of N95 FFRs for single-user reuse for a maximum of 2 decontamination cycles. In a single-user reuse process, the decontaminated FFR goes into a large pool and can be used by anyone.

CDC guidance for disinfection or sterilization in health care facilities states that "In preliminary studies, H₂O₂ vapor decontamination has been found to be a highly effective method of eradicating MRSA, *Serratia marcescens, Clostridium botulinum spores and Clostridium difficile* from rooms, furniture, surfaces and/or equipment; however, further investigation of this method to demonstrate both safety and effectiveness in reducing infection rates are required." (Rutala et al. 2019). An FDA-supported study by Battelle (2016) found that Bioquell HPV, with the established decontamination cycle parameters, achieved a 6-log reduction in organism viability and maintained high filtration and low resistance to air-flow of N95 FFRs following exposure to up to 50 cycles of HPV/VPHP decontamination.

3. Mode of Action

HPV methods are used for terminal decontamination of hospital rooms, biosafety cabinets, and medical equipment and materials that are intolerant to heat or have diffusion-restricted space. Sterilizing units use liquid H_2O_2 that is vaporized or aerosolized and released into the room or chamber. Individual, unwrapped, contaminated objects are placed in a room or biosafety cabinet. Typically, HPV treatment involves a conditioning phase to change room humidity (dry or wet treatment); a gassing phase to saturate the room with hydrogen peroxide gas or vapor (approximately 15 min); a dwell phase to maintain a constant concentration (approximately 125 min); and an aeration or clearance phase during which HPV is converted to oxygen and water vapor (approx. 2–6 h). In this process, inactivation of microorganisms and viruses is achieved primarily by the combined actions of H_2O_2 gas and the generation of hydroxyl and hydroperoxyl free radicals (Finnegan et al. 2010).

There are multiple technologies that do not boil the liquid H_2O_2 solution but rather use a nebulizer to convert the solution into microdroplets. These microdroplets are then distributed into the space in an aerosolized liquid that forms via a visible wet fog. Some percentage of the microdroplets evaporate and achieve equilibrium with the environment, forming a combination of liquid aerosol and vapor phase H_2O_2 . Viral inactivation is achieved through deposition of the liquid microdroplets and condensation of the vapor onto surfaces.

HPGP systems (e.g, STERRAD) and iHP (e.g., SteraMist) use ionization to accelerate the generation of hydroxyl radicals and are used in hospitals for rapid sterilization of BSCs and surgical tools. The gas plasma penetrates the material even when bagged in Tyvek pouches, and also rapidly eliminates any condensed H_2O_2 . The FDA EUA limits STERRAD decontamination of N95 FFRs to a maximum of 2 decontamination cycles.

4. SARS-CoV-2 and Other Pathogen Inactivation

HPV, VHP[™], HPGP and iHP destroy influenza viruses and other viruses and pathogens that are more resistant than SARS-CoVs, such as spores from *G. stearothermophilus*, nosocomial *C. difficile*, and *mycobacterium tuberculosis* (Heckert et al. 1997; EPA, 2004; Hall et al. 2007; Rudnick et al. 2009; Battelle, 2016; Jiang et al., 2017; *Kenny et al. 2020;).

Three recent pre-publications demonstrated that VHP[™] inactivates SARS-CoV-2. Kumar et al. (2020) inoculated four N95 models (3M 1860, 3M 1870, 3M 1804, AO 1054) with SARS-CoV-2 and vesicular stomatitis virus Indiana serotype (VSV). VHP[™] (ARD system, Steris, peak H2O2 concentration >750 ppm) inactivated both SARS-CoV-2 and VSV on all FFR inoculated cutouts (*Kumar et al. 2020). Oral et al. (*2020) inoculated cutouts of N95 (3M 1860S, N=3) with SARS-CoV-2 and treated the cutouts with VHP[™] (Steris LTS-V ARD1000) at 410 ppm for three hours; the treatment inactivated SARS-CoV-2. Fischer et al. (2020) inoculated cutouts from N95 (AO N9504C) with SARS-CoV-2 and treated the cutouts with VHP (1000 ppm, process not identified) for 10 min; the treatment inactivated SARS-CoV-2.

The Dutch National Institute for Public Health report (March 16, 2020) stated that 3M 8822 FFRs treated with HPGP (STERRAD NX100, Express cycle with AllClear[™]) did not support SARS-CoV-2 growth when in medium for 72 hours. HPGP (STERRAD 100NX applied for a standard 47 minute cycle) also inactivated VSV on all FFR inoculated cutouts (*Kumar et al. 2020).

Bergman et al. (2010) studied six different N95 FFRs (industrial N95: 3M 8210; 3M 8000; Moldex 2200 and surgical N95 FFRs: KC PFR95-270; 3M 1870; 3M 1860; N=6 for each of the models tested; FFRs models listed in Bergman et al. (2011)) and applied 3 cycles of decontamination using HPV. The HPV decontamination method (Clarus RTM, Bioquell) involved a gassing phase of 15 min, a dwell phase of 125 min in a 64 m³ room to achieve a room concentration of 8 g/m³ (5700 ppm). After each treatment, a 6-log spore reduction was measured using a biological indicator of *G. stearothermophilus* spores placed inside the room.

The 2016 Battelle Report, prepared for the FDA, summarized a study on the effects of HPV on N95 filter quality and microorganism attenuation. In Phase 1 of the study, HPV treatment (Clarus C^{TM} , Bioquell) of a 20 min gassing phase (2 g/min) followed by a 150 min dwell phase (0.5 g/min) completely inactivated *G. stearothermophilus* spores inoculated by droplet or aerosol onto N95 FFRs (3M 1860). The authors further showed that decontamination was achieved across 50 cycles of repeated treatments. Although the N95 FFRs were shown stacked up against each other in the exposure chamber (Figure 11, Battelle 2016), this resulted in variable sensor readings and is not recommended (personal communication, B. Heimbuch).

Kenny et al. (*2020), in a non-peer reviewed report, evaluated viral decontamination of HPV (BQ-50, Bioquell) after inoculating N95 FFRs (3M 1870) with three different types of aerosolized bacteriophages. A single cycle of HPV completely eradicated phages from the N95 FFRs. N95 FFRs were suspended by their elastic strap on racks in a 33 m³ room for a 30–40 min gas phase at 16 g/min, a 25 min dwell phase, and a 150 min aeration phase.

A not yet peer-reviewed study in a Boston hospital (*Cramer et al., 2020) found that the standard *G. stearothermophilus* spore biological indicator, when placed under or near N95 FFRs in a SteraMist-equipped room that had iHP mist delivered to a total of 90 mL/min for 15 min for a concentration of 17.7 mL/m³, showed an inactivation of > 6-log.

Derr et al. (*2020), in a non-peer reviewed report, evaluated viral decontamination using the Curis aHP system on five models of N95 FFRs (3M 1860, 1870+, 8511, 9211+ and Honeywell Sperian N11125) inoculated with herpes simplex virus 1, Coxsackie virus B3, and phage phi6. If the decontamination room HP exposure killed the biological index (G *stearothermophilus*) then all viruses were inactivated to > 6-log.

Heckert et al. (1997) inoculated glass and stainless steel with 9 exotic animal viruses. After VHPTM treatment, virus titer was reduced to 0 (except for hog cholera virus in whole blood). A VHP 1000 Steris machine was used to generate a gas phase of 2 g/min for 30 min to maintain a H_2O_2 concentration of 1.73 mg/L (1211 ppm).

5. Integrity of N95 Filtering Facepiece Respirators

As noted, there are a variety of H_2O_2 methods and equipment available, and the methods evaluated to date, HPV/VPHP, HPGP, and VHPTM have different effects on N95 filter function. Filter function can be assessed with a quantitative fit test (e.g., PortaCount) or the NIOSH method (e.g. TSI 8130) which quantifies filter efficiency and airflow resistance. The filter efficiency rating for a N95 FFR should be above 95%.

The 2016 Battelle Report phase 2 study evaluated filter quality and fit with Bioquell HPV/VPHP. The same exposure was applied as described above, but with the addition of 300

min of aeration, to 85 N95 FFRs (3M 1860) for 10, 20, 30, 40 and 50 cycles of decontamination, 15 N95 FFRs per cycle set. After decontamination, both inert and bioaerosol collection efficiency remained >99% and no degradation of airflow resistance was found for any of the 85 N95 FFRs (NIOSH method). Mannequin fit quality did not degrade when tested up to 20 cycles of decontamination (no fit testing was done beyond 20 cycles). After 30 cycles, strap degradation was observed with strap length elongation and loss of elasticity, which could negatively impact FFR fit. Only the 3M 1860 N95 model was tested.

The Duke University & Health HPV system (*Schwartz et al., 2020) incorporates results from the Battelle study. N95 FFRs (3M 1860) were either suspended by their elastic straps or layed individually onto stainless steel racks in a disinfection room (12 X 12 ft) of their NIAID Regional Biocontainment Laboratory. The room was treated with HPV (Bioquell Clarus[™] C system with a 35% H₂O₂ solution) to attain a 480+ ppm concentration of HPV with a gas time of 25 min and dwell time of 20 minutes. One hundred N95 FFRs (3M 1860) were treated with HPV for 1 cycle. Air concentration near the N95 FFRs was measured during the aeration period to determine the time when the concentration was below the OSHA Permissible Exposure Limit (1 ppm, 1.4 mg/m³). At 4 hours, the concentration was below the limit of detection (0.2 ppm) of the device (PortaSens IITM sensor). A qualitative test was conducted on the N95 FFRs by 3 individuals who detected no noticeable odors. There was no physical nor performance (not described) degradation of the N95 FFRs. They are currently evaluating the Bioquell Z-2 and Bioquell ProteQTM system with >10 repeated treatment cycles for fit.

Bergman et al. (2011) found that three cycles of HPV decontamination (Bioquell) did not compromise filter efficiency (> 98%) in the six different N95 models tested (see above) nor were there observable physical changes to the N95 FFRs. Although no measurements of filter performance were made in the Kenny et al. (*2020) study, after 5 cycles of HPV treatment, the 3M 1870 N95 FFRs "appeared similar to new with no deformity." Fischer et al. (*2020) evaluated an N95 FFR (3M 9211) with 2 h of wear and VHP decontamination, for 3 rounds and found no decline in quantitative (PortaCount) fit testing.

Viscusi et al. (2009) evaluated six different N95 FFRs (same FFRs as Bergman et al. 2011) and applied one cycle of treatment of HPGP (STERRAD 100S 55-min short cycle, with FFRs in Tyvek pouches) and found no effect on filter efficiency. However, in a follow up study by the same research group, three cycles of HPGP decontamination reduced filtering efficiency by > 5% for 4 of 6 different FFRs tested (NIOSH method; TSI 8130) (Bergman et al. 2010). This is below the FDA-required 95% threshold.

Kumar et al. (*2020) treated 4 different N95 models (3M 1860, 3M 1870, 3M 1804, AO 1054) with multiple cycles of HPGP (STERRAD 100NX 47 min). After 1 cycle of HPGP treatment, qualitative fit testing (PortaCount) demonstrated no reduction in filter quality. However, after 5 cycles of treatment, all 4 FFRs failed qualitative fit testing. The Dutch National Institute for Public Health report (March 16, 2020) summarized the effects of decontamination of 3M 8822 FFRs with up to 4 cycles of HPGP (STERRAD NX100, Express cycle with AllClear™). One or 2 cycles of decontamination did not deform FFRs or compromise fit (qualitative PortaCount method), but 3 cycles compromised fit and 4 cycles deformed the FFRs.

Oral et al. (*2020) treated N95 FFRs (3M 1860S, N=5) with a single cycle of VHP[™] and found no reduction in filter efficiency. Kumar et al (2020) also used VHP[™] (ARD Steris) to treat 4 different N95 FFRs (3M 1860, 3M 1870, 3M 1804, AO 1054). They found no degradation of filter fit test (PortaCount) after 1, 3, 5, or 10 cycles of treatment.

Cramer et al., (*2020) treated N95 FFRs for 5 cycles (3M 1860, N=3 and Halyard 46767, N=3) or 2 cycles (Gerson 2130, N=1 and 3M 8210, N=2) of SteriMist iHP room decontamination. Filter efficiency remained above 97% in all cases. They also tested 3M 1860 and Halyard 46767 and found no degradation in quantitative fit testing after 5 cycles. UCSF (personal communication, 2020) treated 3M 1860 and Halyard Fluidshield N95 FFRs with 0, 1, 2, and 5 cycles of decontamination with Halosil fogger. Filter efficiency remained above 95% after all treatments.

6. Data Summary Tables

| Author | Media | Dose | Phase Times (min) | Strain(s) | Effectiveness (log reduction) |
|--------|---|---|------------------------|---|----------------------------------|
| A | Biological indicators in room (N=5) | HPV (Bioquell) (8 g/m ³ | gas 15; dwell 120 | G stearothermophilus spores | ≥6 |
| В | 3M 1860 N95 FFRs inoculated with aerosol (N=15) | HPV (Bioquell) 2 g/min then 0.5 g/min | gas 20; dwell 150 | G stearothermophilus spores | ≥6 |
| С | 3M 1860 N95 FFRs inoculated with droplets (N=3) | HPV (Bioquell) 2 g/min then 0.5 g/min | gas 20; dwell 150 | G stearothermophilus spores | ≥6 |
| D | 3M 1860 N95 FFRs inoculated with aerosol (N=5) | HPV (Bioquell) 2 g/min then 0.5 g/min | gas 20; dwell 150 | G stearothermophilus spores | ≥6 |
| E | Biological indicators near N95 FFRs (N=30) | SteraMist (TOMI) | gas 15; dwell 20 | G stearothermophilus spores | ≥6 |
| F | 3M 1860 inoculated N95 FFRs (N=3 for each phage) | HPV (Bioquell) 16 g/min | gas 30–40; dwell 25 | Phage phi-6 Phage T7 Phage T1 | ≥6 |
| G | 3M 1860, 1870, 1804 and AO 1054 FFRs (N=1) inoculated with VSV and SARS-CoV2 | VHP [™] (Steris) 5 g/min then 2.2 g/min | gas 3; dwell 30 | Vesicular stomatitis virus; SARS-CoV-2 | ≥6 |
| Н | 3M 1860S FFR pieces inoculated with SARS-CoV2 | VHP [™] (Steris) 410 ppm | 3 h | SARS-CoV-2 | ≥6 |
| I | AO N9504C FFR pieces inoculated with | VHP 1000 ppm | 10 min` | SARS-CoV-2 | ≥6 |

Table 1. Impact of H2O2 decontamination methods on G. stearothermophilus spores and viruses

| | SARS-CoV2 | | | | |
|---|--|---------|---------------------|--|----|
| J | 3M 1860, 1870+, 8511, 9211, HW N11125 FFRs inoculated with virus species | Curis | gas 12; dwell 50 | Herpes Simplex Virus 1 Coxsackievirus B3 Phage phi6 | ≥6 |
| к | Glass and stainless steel inoculated with 9 viruses | 2 g/min | gas 30 | Avian influenza African swine fever virus Bluetongue virus Hog cholera virus Newcastle disease virus Pseudorabies virus Swine vesicular disease virus Vesicular exanthema virus Vesicular stomatitis virus | ≥6 |

A: (Bergman et al., 2010), B: (Battelle, 2016) Phase 1 aerosol inoculated filters, C: (Battelle, 2016) Phase 1 droplet inoculated filters, D: (Battelle, 2016) Phase 3 aerosol inoculated filters, E: (*Cramer et al., 2020), F: (*Kenny et al., 2020), G: (*Kumar et al. 2020), H: (*Oral et al. 2020), I: (*Fischer et al. 2020), J: (*Derr 2020), K: (Heckert et al. 1997).

| Author | N95 FFRs | Dose | Time (min) | # cycles | Filtration efficiency | FFR damage |
|--------|--|---|----------------------|-----------------------|--|--|
| L | 6 different N95 FFR models (N=6 for each model) | HPGP (STERRAD 100S) | 55 | 1 | >99.2% | Not evaluated |
| М | 6 different N95 FFR models (N=6 for each model) | HPV (Bioquell) 8 g/m ³ | gas 15; dwell 120 | 3 | >97% | None noted |
| М | 6 different N95 FFR models (N=6 for each model) | HPGP (STERRAD 100S) | 55 | 3 | <95% (4 of 6 models of N95 tested) | Not evaluated |
| N | 3M 1860 FFRs (N=85 total) | HPV (Bioquell) 2 g/min then 0.5 g/min | gas 20; dwell 150 | 10, 20, 30, 40, 50 | >99% | > 30 cycles, straps fragmented when stretched |
| 0 | 3M 1860S FFRs (N=5) | VHP [™] (Steris) 410 ppm | 3 h | 1 | >98.8% | |
| Р | 3M 1860, Halyard Fluidshield N95 FFRs | Halosil | gas 15; dwell 120 | 0, 1, 2, 5 | >99.3 (3M) >95.5 (HF) | |

| Table 2. Impact of H2O2 decontamination methods on N95 FFR filter efficiency by NIOSH method | Table 2. Impact of H2O2 | decontamination met | hods on N95 FFR fi | Iter efficiency by | v NIOSH method |
|--|-------------------------|---------------------|--------------------|--------------------|----------------|
|--|-------------------------|---------------------|--------------------|--------------------|----------------|

L: (Viscusi et al. 2009), M: Bergman et al., 2010), N: (Battelle, 2016), O: (*Oral et al. 2020), P: (UCSF, personal comm.)

7. Strategies

Commercial systems are available from companies such as ASP, Bioquell, Steris, Battelle, Curis, TOMI, and Halosil, most of which differ in the method of delivering and sustaining H_2O_2 concentrations in aerosolized liquid, vapor or gas plasma phases by temperature, humidity, and the solvents used. Bioquell uses the term hydrogen peroxide vapor (HPV) and Battelle uses the term vapor phase hydrogen peroxide (VPHP) for the same method, Steris uses the term vaporized hydrogen peroxide (VHPTM) for a slightly different method. ASP (STERRAD) applies a different method termed hydrogen peroxide gas plasma (HPGP).

The Bioquell wet-HPV systems [used by Duke, Bergman et al. (2010) and Battelle (2016)] includes a generator to produce HPV, a module to measure the concentration of HPV, temperature, and relative humidity in the enclosure, and an aeration unit to catalyse the breakdown of HPV into oxygen and water vapor after HPV exposure. The Bioquell systems do not control the H_2O_2 air concentration. HPV is delivered until the air in the enclosure becomes saturated and H_2O_2 begins to condense on surfaces (Hall et al., 2007; Ray et al., 2010). The manufacturer uses RFID-chipped bottles with a 35% peroxide solution without additives. It is important that such high concentrations of peroxide be handled safely; high concentrations are toxic irritants and, under certain circumstances, explosive.

The Steris dry-VHPTM systems have a generator inside the room with an integral aeration unit and dehumidifier to a set humidity level prior to the start of the cycle. The system delivers 'non-condensing' VHPTM by drying the vapor stream as it is returned to the generator. The Steris systems monitor the H₂O₂ air concentration throughout the exposure period.

The STERRAD system (ASP) generates a H_2O_2 gas plasma (HPGP) from HPV with radiofrequency (RF). In this process, HPV inactivates virus and other pathogens and RF converts HPV to plasma which converts rapidly to water and carbon dioxide. The HPGP process reduced N95 filter efficiency with 3 cycles of decontamination in at least some studies (Bergman et al., 2010). It is not known why the HPGP process, compared to other HPV processes, reduces N95 filter efficiency. One possible explanation is that the RF directly impacts the electrostatic properties of the polypropylene electret filter (Dr. Peter Tsai, personal communication).

The Curis® system uses a solution of 7% hydrogen peroxide with a proprietary blend to create a fog of aerosolized liquid H_2O_2 and vapor with concentration between 80-150 ppm. The aerosolized droplets form a micro-condensation which contributes to the efficacy of the process. This treatment is based on delivery of solution combined with microdroplets within the treatment area. Although the manufacturer of the system has internal studies showing a 6-log reduction of *G. stearothermophilus* spores in HEPA and N95 applications and no failures in fit testing, its impact on filtration efficiency is unknown (*Derr et al., 2020).

The Halo system (Halosil) aerosolizes hydrogen peroxide (aHP). It uses the HaloMist solution which contains a low percentage (5%) hydrogen peroxide with a biocidal silver nitrate additive at a low concentration (0.01%). Halo foggers generate a 100-120 ppm H_2O_2 vapor content through initial water evaporation from microdroplets that concentrate both the peroxide and the silver. This effectively increases the peroxide concentration in the vapor phase above the initial 5%. It is not known whether the low silver nitrate concentration

negatively impacts the electrostatically-charged filter of N95 FFRs. An independent 3rd party study is underway to assess this.

The Battelle process involves the hospital collecting FFRs labeled with hospital number, unit number (and user name), shipping them to one of 6 sites around the country, processing them and returning them to the same hospital. Up to 80,000 FFRs can be processed per day at one site. Turn around is approximately 10 days.

The Duke Medical Center has developed a procedure for decontaminating N95 FFRs using the Bioquell Clarus[™] C system and has performed qualitative testing on more than one hundred N95 FFRs (see above; *Schwartz et al., 2020). Soiled N95 FFRs with visible blood, hair or damage are discarded and not decontaminated. N95 FFRs are separated into 4 streams based on size of N95 FFR (common: 3M 1860 or small: 3M 1860s) and the visible presence or absence of facial cosmetics. After decontamination, the integrity of the straps (evaluate for elongation), nose bridge, and nose foam are checked for integrity. The Duke Medical Center protocol does not return the FFRs back to the same user while the Battelle protocol can depending on how the hospital manages the FFRs. N95 FFRs are fit to a person's face and fit tested to confirm that there is no side leakage. A theoretical benefit of returning the FFR to the same user is to preserve the fit. When users receive their decontaminated N95 FFRs they should don the FFR and perform a self seal check to ensure that there is no side leakage.

8. Primary Risks and Unknowns

Dosing protocols are complex and could result in incomplete decontamination. Standard spore attenuation tests can be incorporated during decontamination. H_2O_2 is a strong oxidizer that can be an explosion hazard under certain conditions. Therefore, only trained personnel should operate HPV, VHPTM or HPGP equipment. H_2O_2 gas is a corrosive irritant that can cause skin, eye and lung damage. H_2O_2 gas may interact with N95 FFR components to form a toxic residue - analytical chemistry tests for H_2O_2 can test for this. The OSHA permissible exposure limit is 1 ppm over an 8-hour Time Weighted Average (TWA). During the decontamination process, room concentrations may be higher than 100 ppm.

Detection of odor does not provide adequate warning of hazardous residual concentrations in the N95 FFRs. Complete off-gassing of sentinel FFRs should be confirmed with quantitative H_2O_2 testing (e.g., PortaSens-II test).

Probability of N95 FFRs straps failure increases with more than 20 cycles of decontamination; this will vary with the decontamination method and N95 FFRs model. Straps should be examined after decontamination and prior to each use to ensure that they are not elongated.

It is important to note that HPV/VPHP, VHPTM and HPGP are not compatible with cellulose, which is not a component listed in 3M model 1860 N95 FFRs but may be present in other FFRs (Appendix A). The presence of cellulose in FFRs is an important consideration in the adoption of H_2O_2 -based strategies.

Repeated donning of a N95 FFR will gradually reduce the fit. For some N95 models a study found that fit declines to below acceptable after 5 donnings and for other models this does not occur until 15 donnings (Bergman et al., 2012).

9. Conclusions

Multiple studies have confirmed that N95 FFRs contaminated with aerosol or droplets containing *G. stearothermophilus* spores were successfully decontaminated with H_2O_2 with a 6-log reduction in spore level. Recent studies confirm that SARS-CoV-2 on N95 FFRs are eradicated with VHPTM (*Kumar et al. 2020; *Oral et al. 2020; *Fischer et al. 2020). N95 (3M 1860) FFRs filter efficiency did not degrade with up to 50 cycles of HPV decontamination. However, after 20 cycles of HPV decontamination the N95 FFRs straps showed degradation and were permanently deformed when stretched. A disadvantage of H2O2 processes is that the N95 FFRs must be completely aerated after treatment and this may take 4 to 8 hours.

Many hospitals already have HPV/VPHP systems in-house for use in full room terminal decontamination. These could be deployed to dedicated N95 decontamination rooms. Processing carts filled with spaced out N95 FFRs could be wheeled in and out of the room. Alternatively, existing biosafety cabinets within the hospital can be connected to a VHPTM or HPV unit. Another solution is to send the FFRs to an outside service-provider (e.g., Battelle) for decontamination. To achieve an appropriate concentration of H_2O_2 vapor during the gas and dwell phase the specification of the HPV system should be matched to the treated volume. The long aeration phase could be conducted in an adjacent room where H_2O_2 vapor is converted to inert O_2 and water vapor. The concentration of HPV should be measured during decontamination to confirm adequate treatment level and also at the end of aeration to protect workers who enter the room. The OSHA Permissible Exposure Limit is 1 ppm (1.4 mg/m³). HPV can be detected by smell and irritation, but may still pose respiratory dangers at levels below user detection.

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Appendix A. List of N95 FFRs with or without cellulose based on information from Battelle and 3M Personal Safety Division (9 April 2020).

| Cellulose-free N95 FFRs listed by Battelle and/or 3M Personal Safety Division |
|---|
| 3M 1860 (+S) |
| 3M 1870+ |
| 3M 8000 |
| 3M 8205 |
| 3M 8110S |
| 3M 8210 |
| 3M 8210+ |
| 3M 8210V |
| 3M 8211 |
| 3M 8211+ |
| 3M 8240 |
| 3M 8246 |
| 3M 8247 |
| 3M 8271 |
| 3M 8511 |
| 3M 8515 |
| 3M 8516 |
| 3M 8576 |
| 3M 8577 |
| 3M 9010 |
| 3M 9210+ |
| 3M 9211+ |
| Gerson 1730 |
| Gerson 2140C |
| Moldex 1500 Series |
| Moldex 2200 |
| Kimberly Clark 46727 |
| Cellulose-containing N95 FFRs listed by 3M Personal Safety Division |
| 3M 9105 (+S) |
| 3M 1804 (+S) |
| 3M 1805 (+S) |
| 3M 8000 |
| 3M 8200 |
| 3M 8212 |
| 3M 8214 |
| 3M 8233 |
| |

3M 8233 3M 8293

3M 8512 3M 8514

3M 9010

3M 9105 (+S)